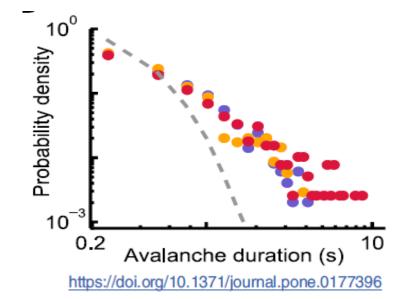
Critical Synchronization Dynamics of the Kuramoto Model on a Large Human Connectome

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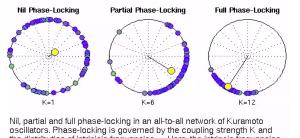
Theoretical research and experiments suggest that the brain operates at or near a **critical state** between sustained activity and an inactive phase, exhibiting optimal computational properties (see: *Beggs & Plenz J. Neurosci. 2003; Chialvo Nat. Phys. 2010; Haimovici et al. PRL 2013)*

Individual neurons emit periodic signals: (Y. Penn et al PNAS 113 (2016) 3341)

→ Critical behavior at the synchronization transition?



Kuramoto oscillator model (1975)



the distribution of intrinisic frequencies ... Here, the intrinsic frequencies were drawn from a normal distribution (M=0.5Hz, SD=0.5Hz). The yellow disk marks the phase centroid. Its radius is a measure of coherence.

Order parameter : average phase:

 $\dot{\theta}_i(t) = \omega_{i,0} + \frac{K}{k_i} \sum_j W_{ij} \sin[\theta_j(t) - \theta_i(t)]$ phases $\theta_i(t)$ in-degrees k_i global coupling K is the control parameter weighted adjacency matrix W_{ij}

 $\omega_{i,0}$ is the intrinsic frequency of the *i*-th oscillator,

$$R(t) = \frac{1}{N} \left| \sum_{j=1}^{N} e^{i\theta_j(t)} \right|$$

Non-zero, above critical coupling strength $K > K_{c}$, Evolves to zero for $K \leq K_{c}$ At $K = K_{\alpha}$ from incoherent initial state : initial growth: $R \sim t^{\eta}$

Critical synchronization transition for D > 4 spatial dimensions, which is mean-field like: i.e. $D \rightarrow \infty$ (full graph)

The dynamical behavior suffers very strong corrections to scaling and chaoticity, see:

Róbert Juhász, Jeffrey Kelling and Géza Ódor: Critical dynamics of the Kuramoto model on sparse random networks J. Stat. Mech. (2019) 053403

Large Human Connectome graphs

Diffusion and structural MRI images with 1 mm^3 voxel resolution : $10^5 - 10^6$ nodes

Hierarchical modular graphs

Top level: 70 brain region (Desikan atlas)

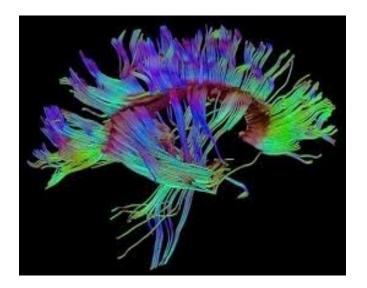
Lower levels obtained by deterministic tractography: FACT algorithm

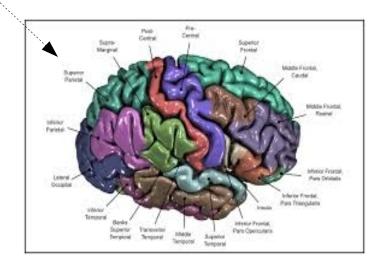
Map : voxel \rightarrow vertex (~ 10⁷)

fiber \rightarrow edge (~ 10¹⁰)

+ noise reduction \rightarrow graph

undirected, weighted





Structural graphs of nodes (containing ~10⁴ neurons) and power-law weight distributed edges see : Michael T. Gastner and Géza Ódor, Scientific Reports 6 (2016) 27249

Kuramoto solution for the KKI-18 graph with *N*= 804 092 nodes and 41 523 908 weighted edges

The synchronization transition point determined by growth from disorder KKI-18 has $D = 3.05 < 4 \rightarrow$

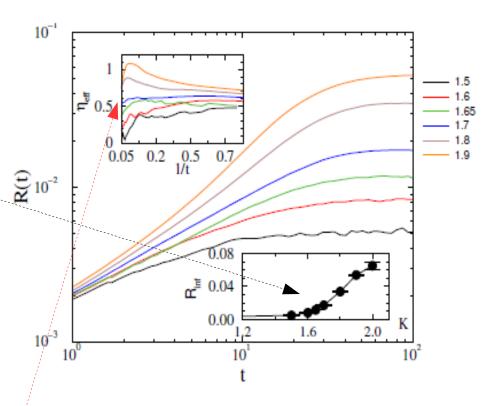
Smooth crossover to partial synch.

Fat-tailed link weight distribution, incoming weight normalization is applied:

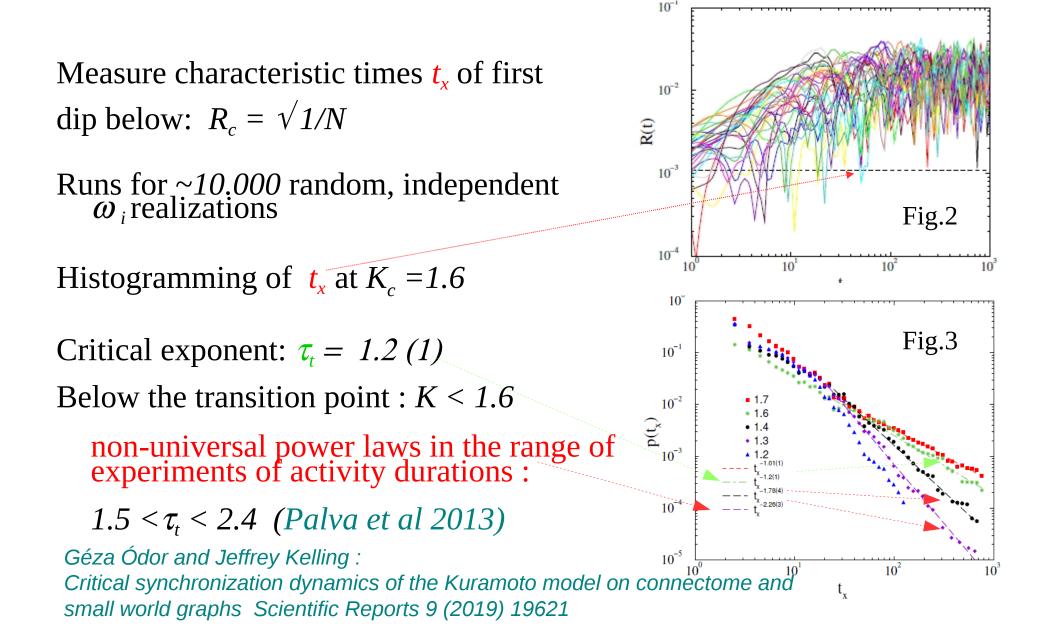
$$W_{i,j}' = W_{i,j}' / \sum_{j \in \text{neighb.of } i} W_{i,j}$$

to provide local homeostasis (suppress hubs)

 $K_c = 1.7$ and growth exponent: $\eta = 0.6(1)$



Determination of the characteristic time exponent: τ_t



The effect of additive stochastic noise

Brain experiments: $\omega_i > 0$, distributions are narrow: $\sigma_i \sim 0.02$ and have mean value: $\langle \omega_i \rangle \sim 0.05$

Galilean invariance of the Kuramoto equation:

 $\langle \omega_i \rangle \neq 0$ can be gauged out by a rotating coordinate system and rescaling of ω_i as : $\omega_i \rightarrow a \omega_i' t \rightarrow (1/a) t' K \rightarrow aK'$ **Existing results can be obtained at later times and weaker K**

Gaussian distributed annealed noise is added:

Conclusions

Heterogeneity effects are simulated on **large** human connectomes This enables us to distinguish from finite size rounding effects Local homeostasis is needed to find criticality

New method to determine crossover to desynchronization and to measure the characteristic times

Below the transition point non-universal dynamical scaling of synchronization \rightarrow Frustrated synchronization in modules

Desynchronization durations exponents τ_t agree in vivo activity experiments for humans

Results are valid for realistic, narrow band ω_i frequency distributions

Insensitivity for weak, additive Gaussian noise

G. Ódor, J.Kelling, G. Deco: accepted in J. Neurocomputing

preprint : arXiv:1912.06018